

# Diffusion posterior sampling: methodology and applications to ECG reconstruction

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Ecole polytechnique

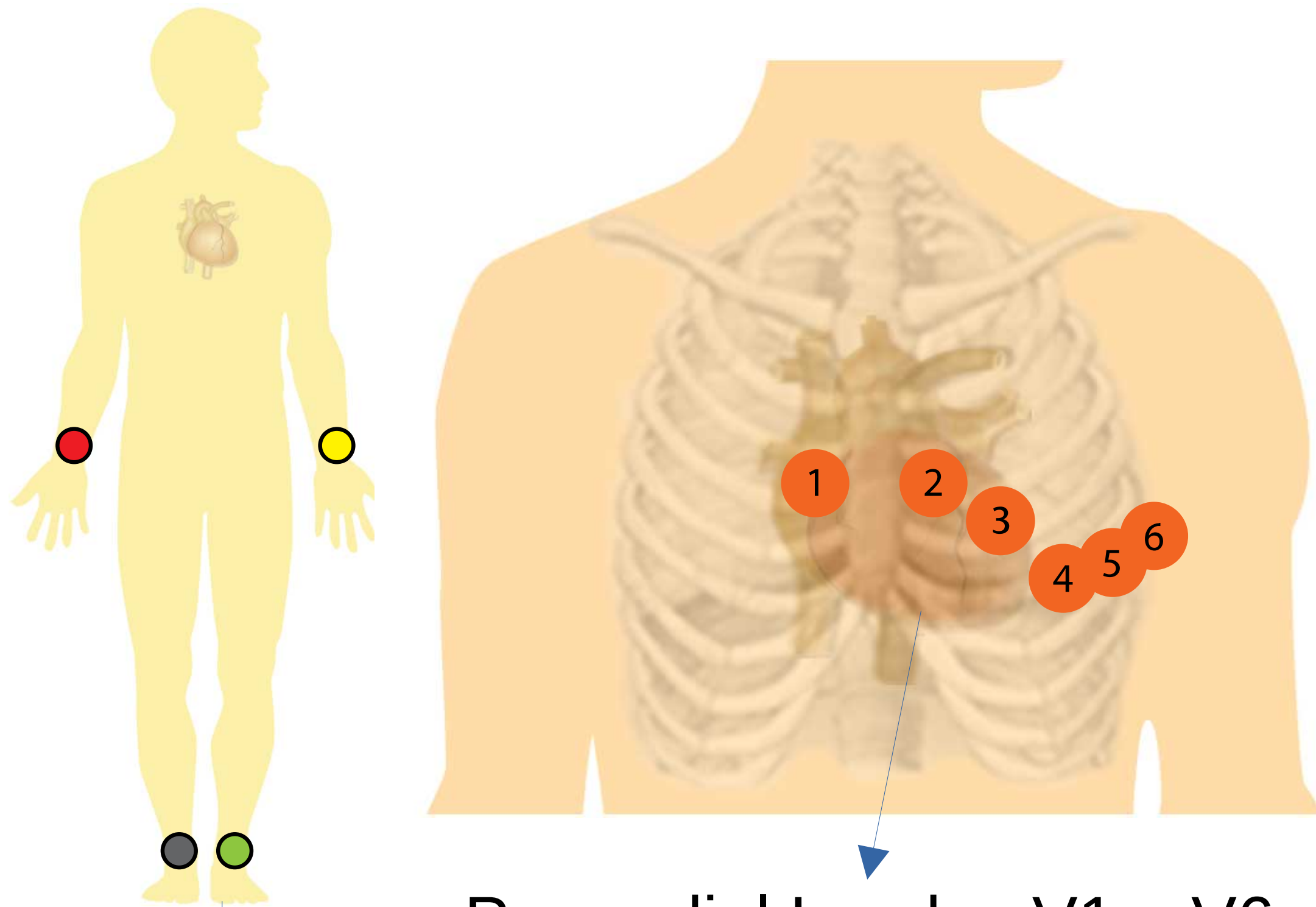
*Joint work with:*

*Yazid Janati, Gabriel Cardoso, Badr Moufad, Alain Durmus, Randal Douc, Jimmy Olsson, Eric Moulines*

# Context

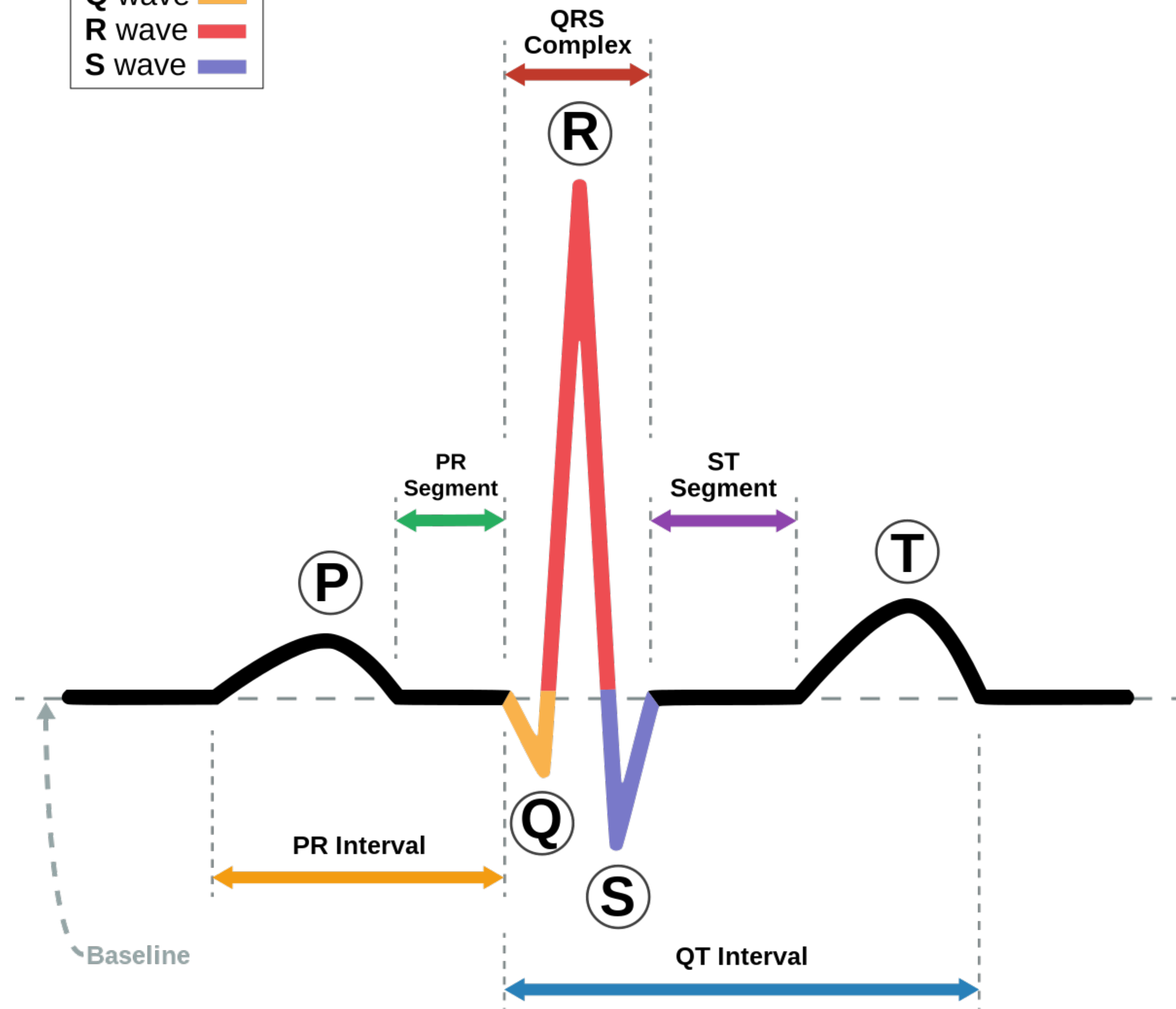
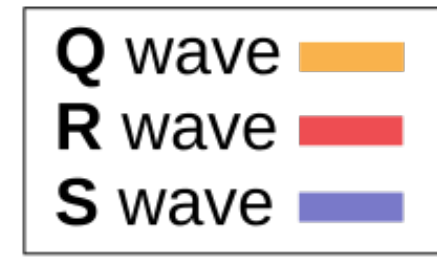
# ECGs

## Electrodes Placement

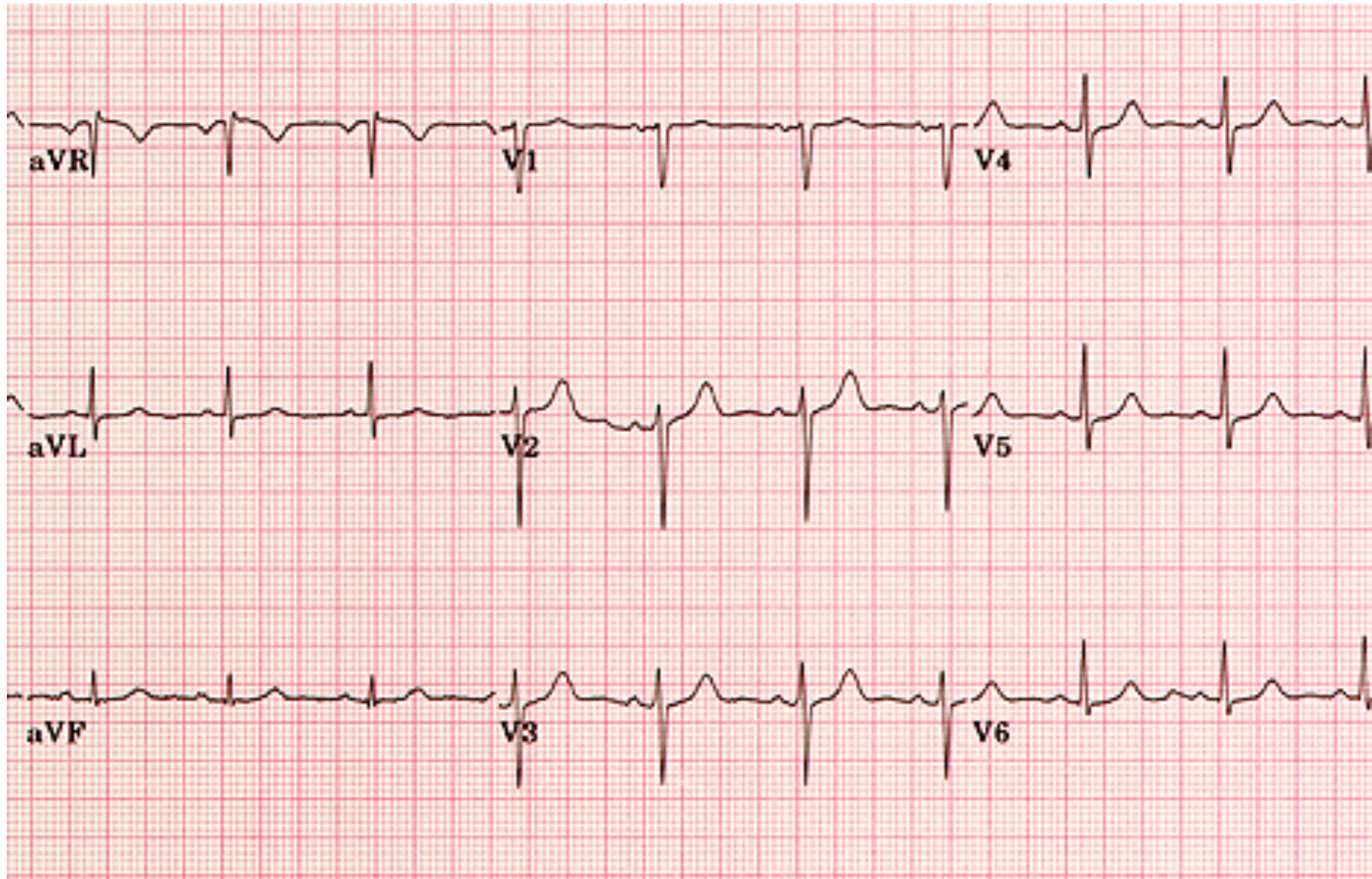


Precordial Leads : V1 – V6  
(closer to the heart)

Limbs Leads :  
aVL, aVR, aVF



# ECGs



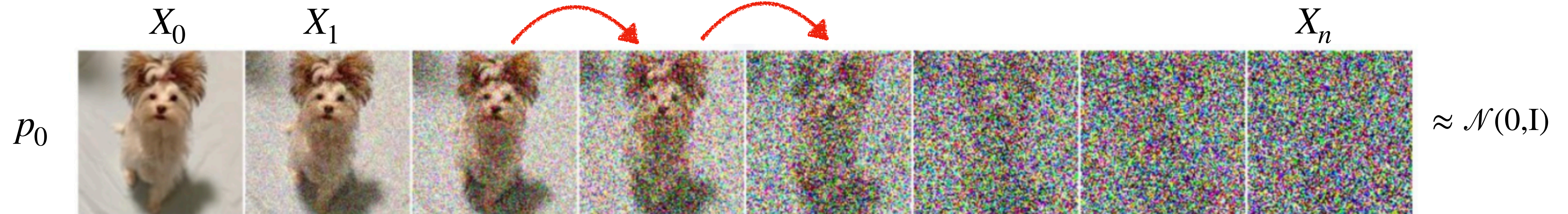
- Acquisition noise : baseline wander, electrode motion
- Incomplete ECG e.g., missing leads in portative devices Kardia, Smart Watch ...

Question : how to recover an ECG from noisy data / from incomplete data ?

# Denoising Diffusion models

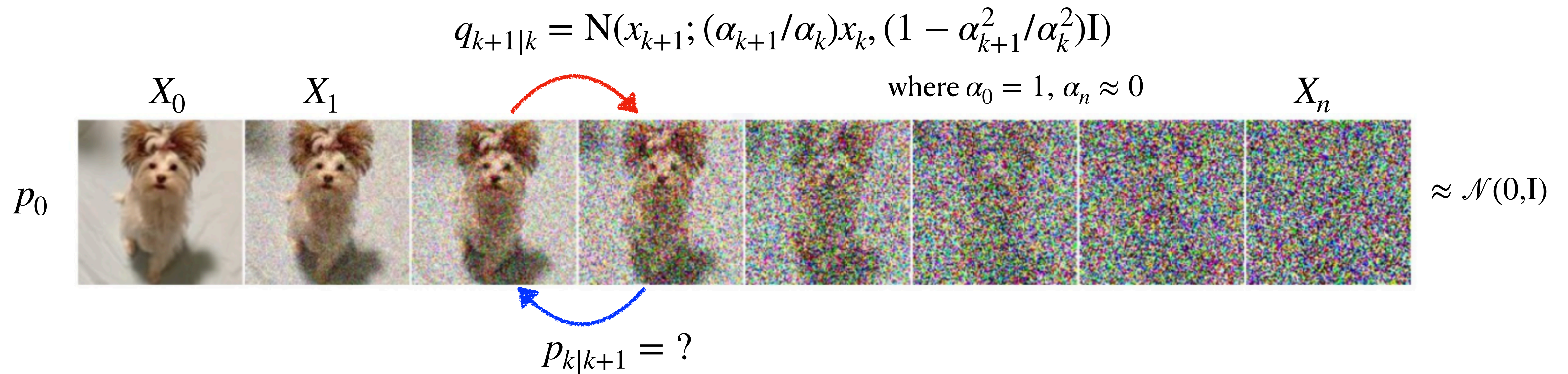
# Diffusion models

Forward noising process

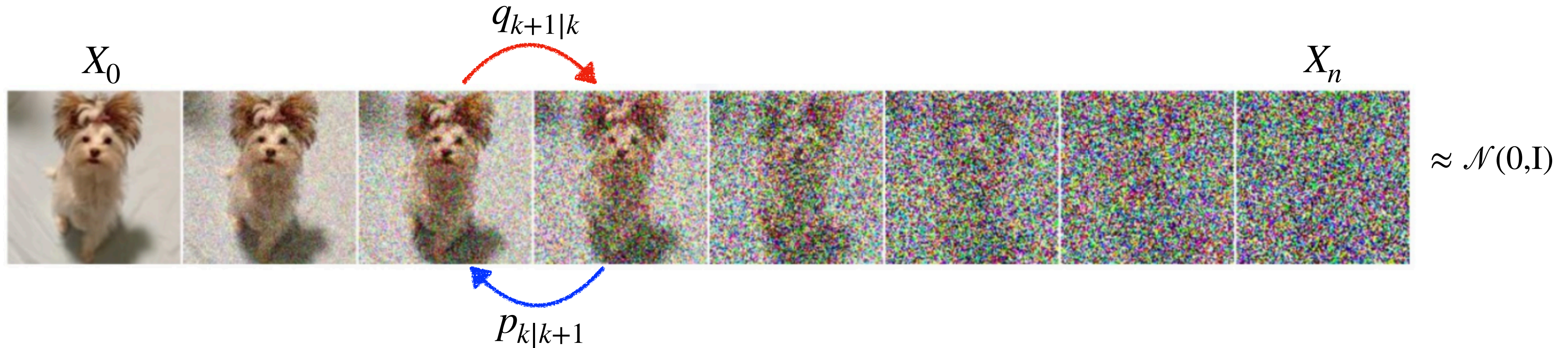


Backward denoising process

# Diffusion models



# Diffusion models



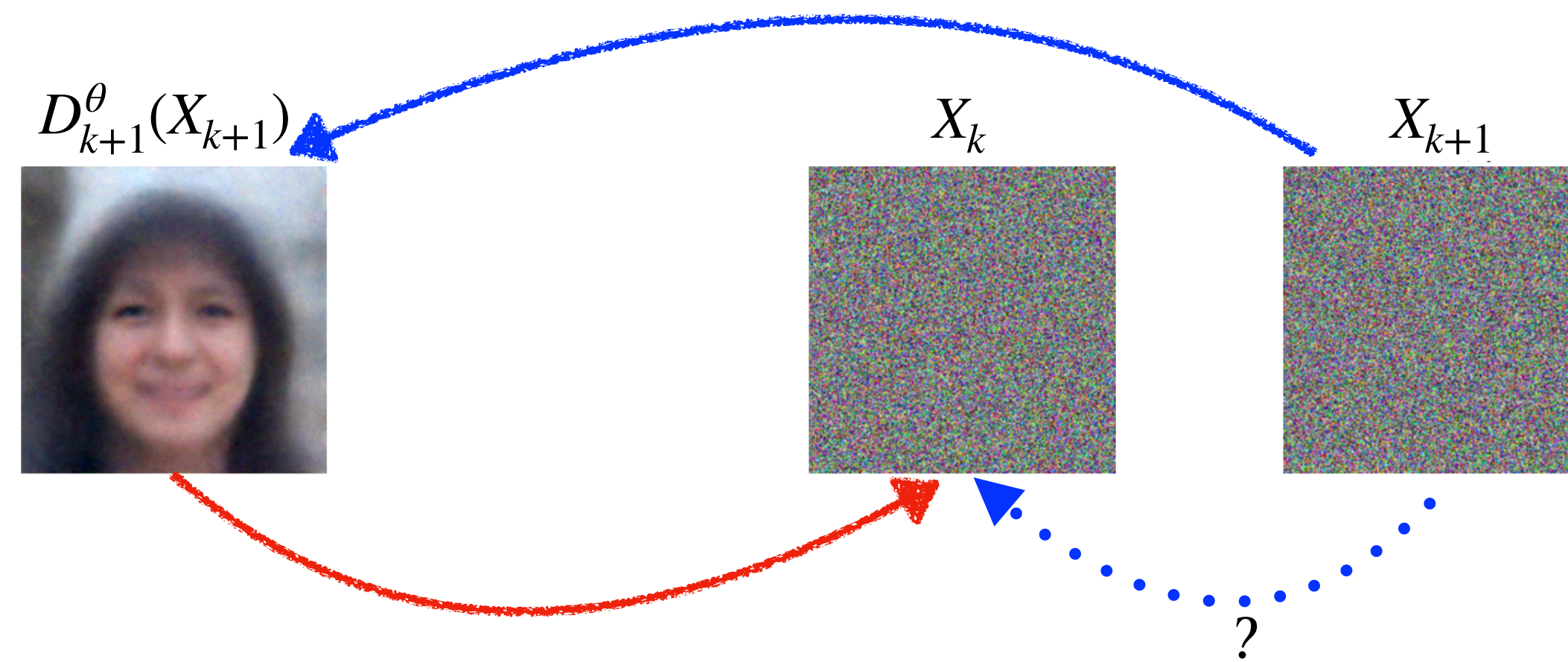
$$\begin{aligned}
 p_{0:n}(x_{0:n}) &= p_0(x_0) \prod_{k=0}^{n-1} q_{k+1|k}(x_{k+1} | x_k) && = \mathbf{N}(x_{k+1}; (\alpha_{k+1}/\alpha_k)x_k, (1 - \alpha_{k+1}^2/\alpha_k^2)\mathbf{I}) \\
 & && \text{where } \alpha_0 = 1, \alpha_n \approx 0 \\
 &= p_n(x_n) \prod_{k=0}^{n-1} p_{k|k+1}(x_k | x_{k+1}) \\
 &\approx \mathcal{N}(0, \mathbf{I}) && \text{intractable}
 \end{aligned}$$



# Diffusion models

$$p_{k|k+1}(x_k | x_{k+1}) = \int q_{k|0,k+1}(x_k | x_0, x_{k+1}) p_{0|k+1}(x_0 | x_{k+1}) dx_0$$
$$\approx q_{k|0,k+1}(x_k | D_{k+1}^\theta(x_{k+1}), x_{k+1})$$

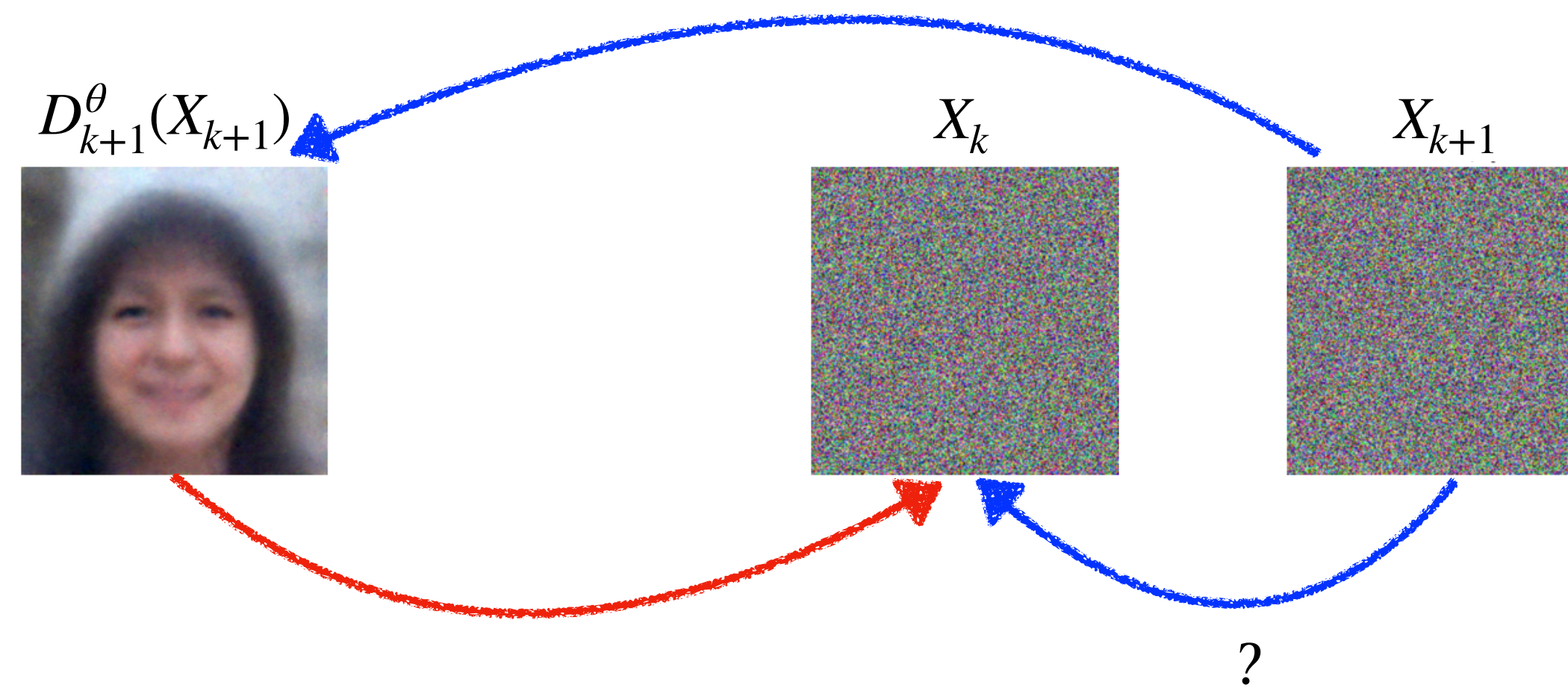
where  $D_{k+1}^\theta$  is a « denoiser » with parameters  $\theta$ , minimizing  $\mathbb{E}[D_{k+1}^\theta(X_{k+1}) - X_0]$



# Diffusion models

$$p_{k|k+1}(x_k | x_{k+1}) = \int q_{k|0,k+1}(x_k | x_0, x_{k+1}) p_{0|k+1}(x_0 | x_{k+1}) dx_0$$
$$\approx q_{k|0,k+1}(x_k | D_{k+1}^\theta(x_{k+1}), x_{k+1})$$

where  $D_{k+1}^\theta$  is a « denoiser » with parameters  $\theta$ , minimizing  $\mathbb{E}[D_{k+1}^\theta(X_{k+1}) - X_0]$

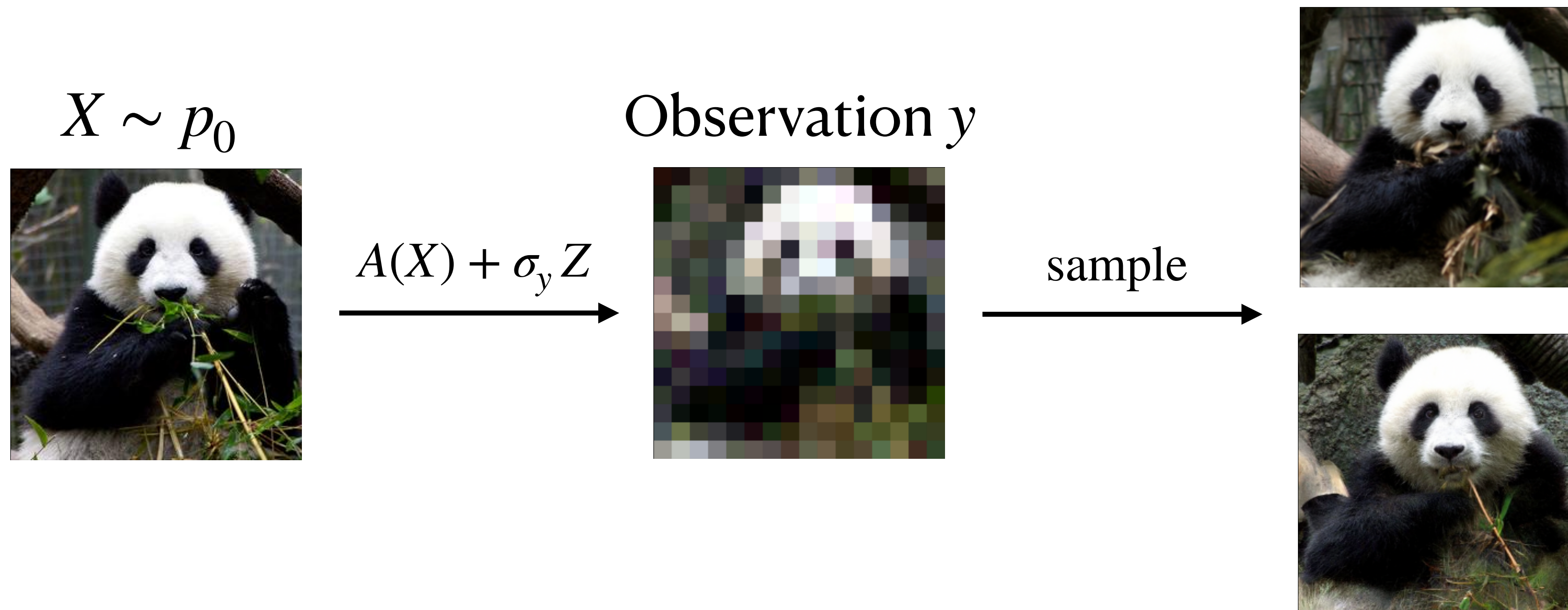


# Bayesian Inverse Problems

# Bayesian inverse problems

$$Y = A(X) + \sigma_y Z, \quad X \sim p_0$$

Given a realisation  $Y = y$ , sample the most **plausible** reconstructions  $X$



# Bayesian inverse problems

The reconstructions are encoded in the posterior distribution

$$\pi_0^y(x) \propto g_0(y|x) p_0(x)$$

where  $g_0(y|x) = \mathcal{N}(y; A(x), \Sigma_y^2)$ .

Sampling plausible reconstructions



Drawing samples from  $\pi_0^y$

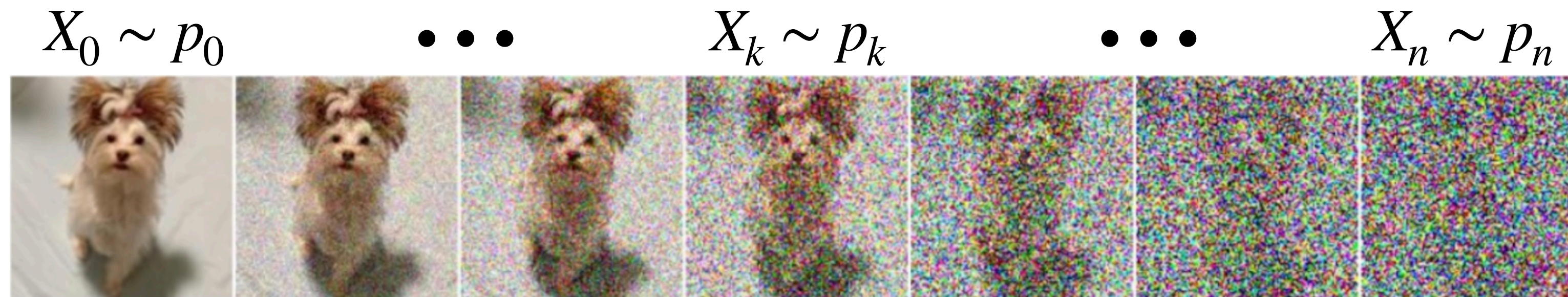
# Diffusion Posterior Sampling

# Diffusion Posterior Sampling

$$\pi_0^y(x) \propto g_0(y|x) p_0(x)$$

Given a **pre-trained** diffusion model  $p_0^\theta \approx p_0$ , develop an efficient algorithm for sampling from  $\pi_0^y$  with no further model training

# Distribution path



$$p_k(x_k) = \int p_0(x_0) q_{k|0}(x_k | x_0) dx_0$$

Diffusion model for  $\pi_0^y \iff$  follow path  $(\pi_k^y)_{k=n}^0$  where

$$\begin{aligned} \pi_k^y(x_k) &= \int \pi_0^y(x_0) q_{k|0}(x_k | x_0) dx_0 \\ &\propto g_k(y | x_k) p_k(x_k) \end{aligned}$$



# Posterior denoiser

Define the likelihood of  $y$  given the noised sample  $x_k$

$$g_k(y | x_k) = \int g_0(y | x_0) p_{0|k}(x_0 | x_k) dx_0$$

We can relate the posterior denoiser  $D_k^y$  to the prior denoiser  $D_k$

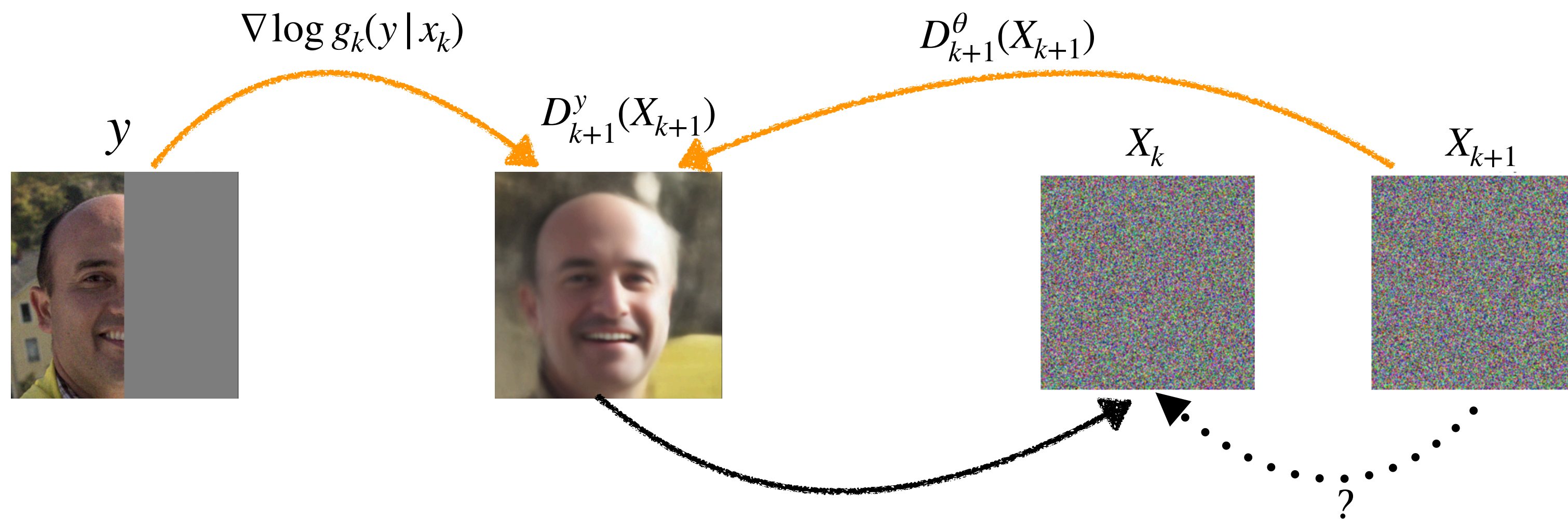
$$D_k^y(x_k) = D_k(x_k) + \alpha_k^{-1}(1 - \alpha_k^2) \nabla \log g_k(y | x_k)$$

$\approx D_k^\theta(x_k)$  ??

# Posterior denoiser

$$D_k^y(x_k) = D_k(x_k) + \alpha_k^{-1}(1 - \alpha_k^2) \nabla \log g_k(y | x_k)$$

$\approx D_k^\theta(x_k)$                       ??



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$\approx D_k^\theta(x_k)$  ??

[Ho, J., Salimans, T., Gritsenko, A., Chan, W., Norouzi, M. and Fleet, D.J., 2022. Video diffusion models.]

[Chung, H., Kim, J., Mccann, M.T., Klasky, M.L. and Ye, J.C., 2022. Diffusion posterior sampling for general noisy inverse problems.]

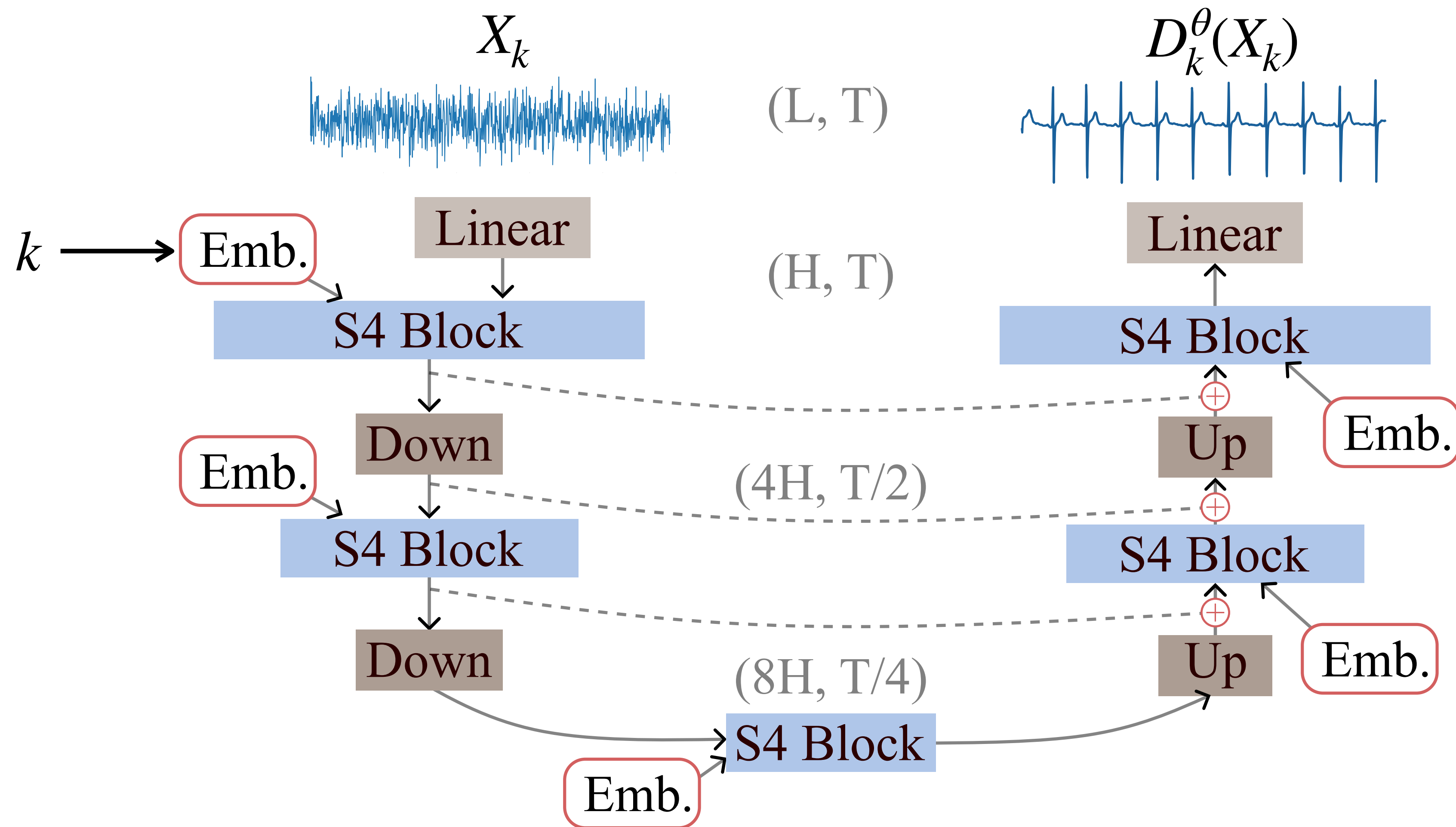
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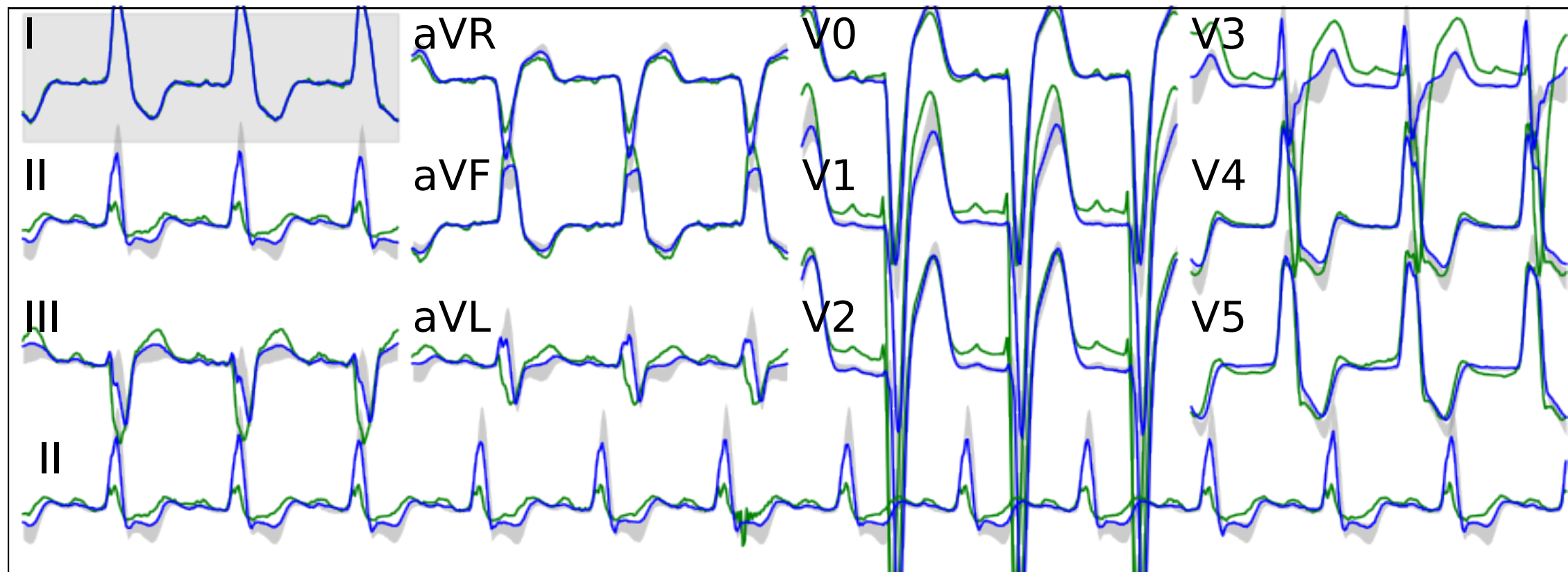
# Applications to ECGs

# Denoiser for ECGs $D_k^\theta$

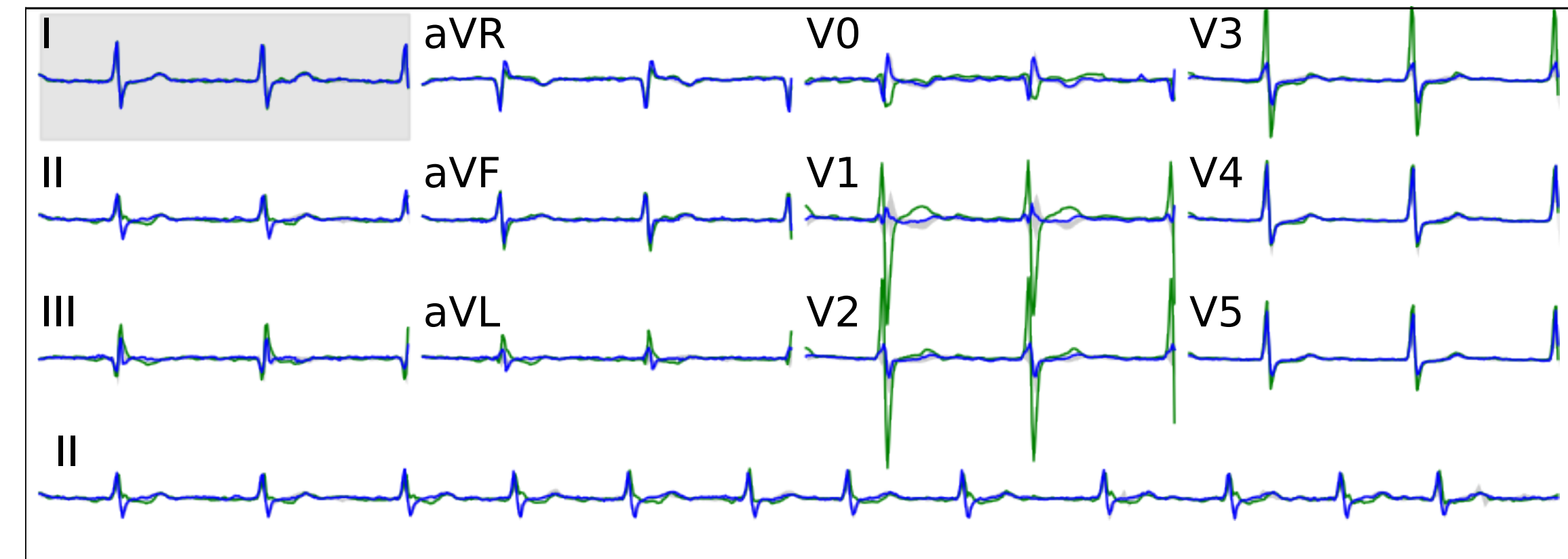


# Reconstruction of Missing Leads

## Bundle Block Branch



## Atrial Fibrillation



Method	Task	RMSE ( $\downarrow$ )	Errors MAD ( $\downarrow$ )	DTW ( $\downarrow$ )	XRESNET1D50 AUC-PR ( $\uparrow$ )		
					NSR	BBB	AF
Ground-truth	-	-	-	-	1.00	1.00	0.98
RhythmDiff-MGPS	MLR	<b>0.19 <math>\pm</math> 0.01</b>	<b>0.09 <math>\pm</math> 0.00</b>	<b>0.29 <math>\pm</math> 0.02</b>	<b>0.99</b>	<b>0.91</b>	<b>0.96</b>
RhythmDiff-DPS	MLR	1.61 $\pm$ 0.17	0.16 $\pm$ 0.01	77.35 $\pm$ 15.34	0.97	0.65	0.68
RhythmDiff-PGDM	MLR	0.19 $\pm$ 0.01	0.10 $\pm$ 0.003	0.32 $\pm$ 0.03	0.99	0.90	<u>0.89</u>
RhythmDiff-DDNM	MLR	0.19 $\pm$ 0.01	0.10 $\pm$ 0.003	0.36 $\pm$ 0.03	0.99	<b>0.92</b>	0.81
RhythmDiff-DIFFPIR	MLR	0.21 $\pm$ 0.01	0.11 $\pm$ 0.003	0.39 $\pm$ 0.03	0.94	0.71	0.57
RhythmDiff-REDDIFF	MLR	0.20 $\pm$ 0.01	0.11 $\pm$ 0.003	0.36 $\pm$ 0.02	0.97	0.87	0.75
ECGRECOVER [26]	MLR	0.34 $\pm$ 0.005	0.20 $\pm$ 0.003	1.10 $\pm$ 0.04	0.98	0.73	0.61

# Artefact Removal in ECGs

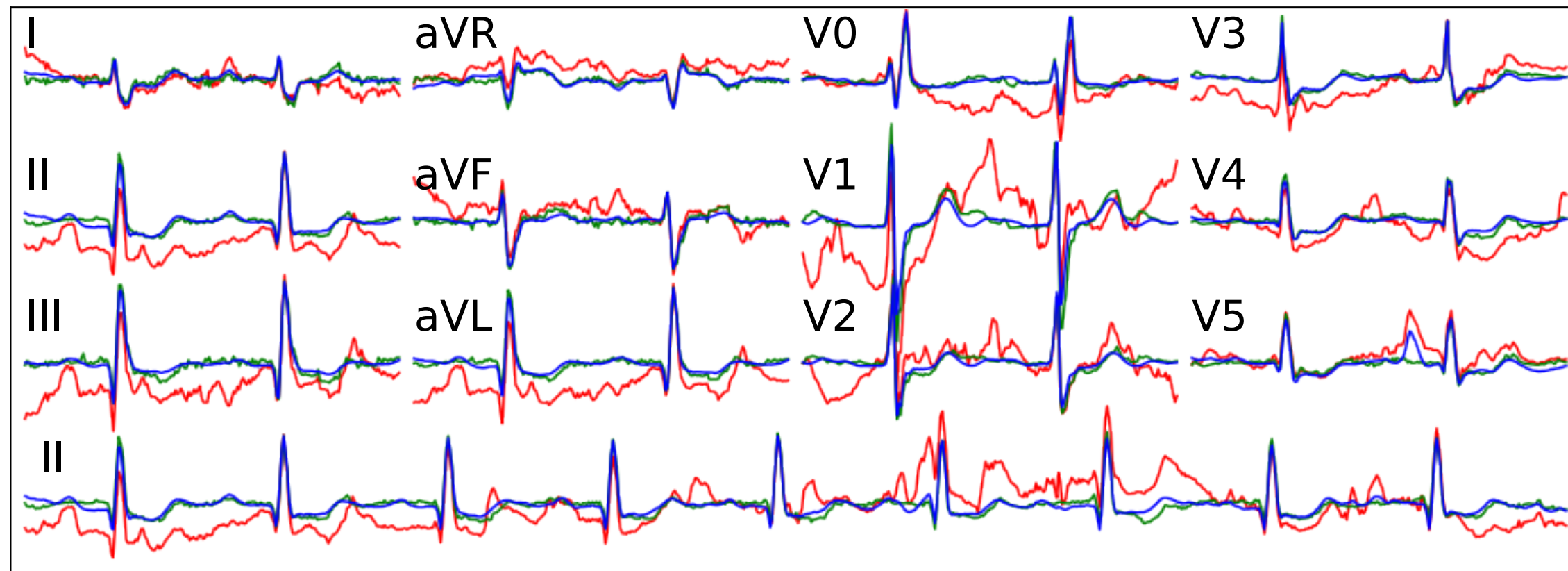
$$Y = X + \sum_{j=1}^J \mu_j \phi_j + \sigma_y Z, \quad X \sim p_0$$

Given  $J$  Fourier harmonics  $\phi_{j \in [1, J]}$  modeling additive artifacts, and a realization  $Y = y$

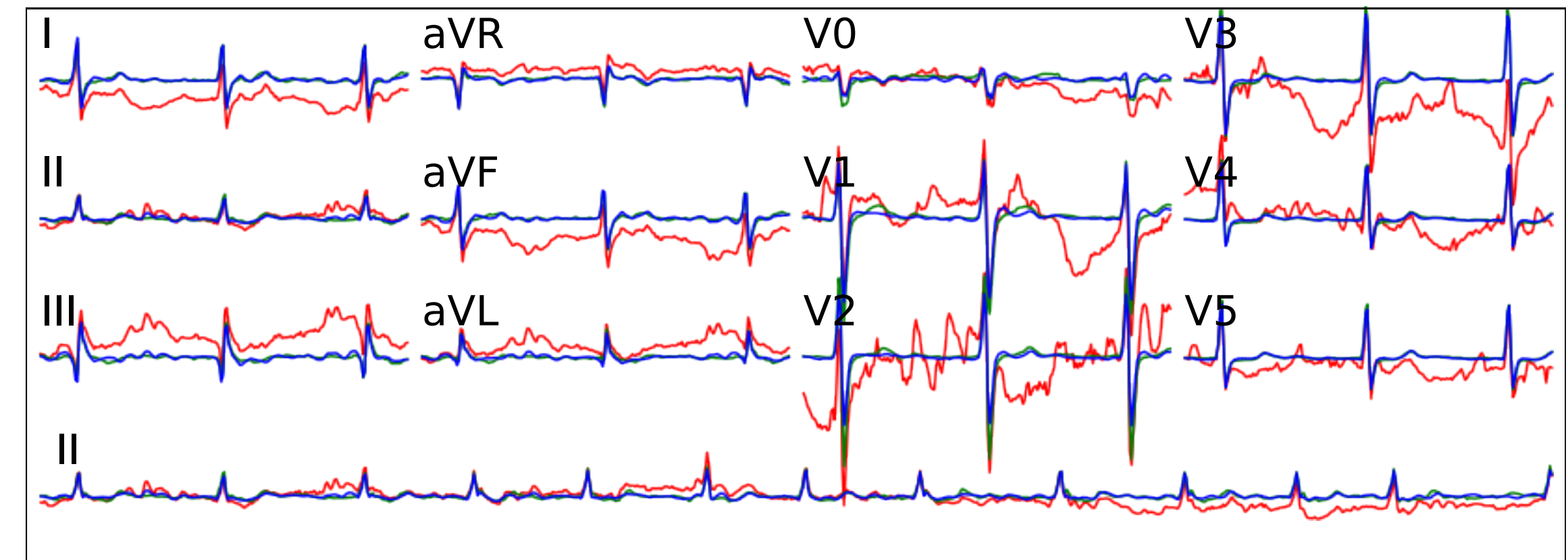
- 1) propose **weights**  $\mu_{j \in [1, J]}$
- 2) sample most plausible reconstruction  $X$
- 3) regress new  $\mu_{j \in [1, J]}$
- ... iterate until convergences

# Artefact Removal in ECGs

## Bundle Block Branch



## Atrial Fibrillation



Method	Task	RMSE ( $\downarrow$ )	Errors MAD ( $\downarrow$ )	DTW ( $\downarrow$ )	XRESNET1D50 AUC-PR ( $\uparrow$ )		
					NSR	BBB	AF
Ground-truth	-	-	-	-	1.00	1.00	0.98
RhythmDiff-MGPS	EMR	<b>0.097</b> $\pm$ 0.002	<b>0.059</b> $\pm$ 0.001	<b>0.13</b> $\pm$ 0.01	<b>1.00</b>	<b>1.00</b>	<b>0.86</b>
DEScOD [29]	EMR	0.100 $\pm$ 0.002	0.074 $\pm$ 0.001	0.13 $\pm$ 0.01	1.00	0.98	0.81
RhythmDiff-MGPS	BWR	0.134 $\pm$ 0.003	0.078 $\pm$ 0.001	0.24 $\pm$ 0.02	0.99	0.97	0.86
DEScOD [29]	BWR	0.088 $\pm$ 0.002	0.062 $\pm$ 0.001	0.11 $\pm$ 0.01	0.99	0.99	0.88



# Conclusion

A single trained diffusion model for multiple downstream task

[Bedin, L., Cardoso, G., Duchateau, J., Dubois, R., Moulines, E., 2024. Leveraging an ECG beat diffusion model for morphological reconstruction from indirect signals.]

[Moufad, B., Janati, Y., Bedin, L., Durmus, A., Douc, R., Moulines, E., Olsson, J., 2025. Diffusion posterior sampling with midpoint guidance.]









# Midpoint Guidance Posterior Sampling

# Posterior denoiser approximation

$$\int g_0(y | x_0) p_{0|k}(x_0 | x_k) dx_0 \approx g_0(y | D_k(x_k))$$

implicitly assumes that  $p_{0|k}(\cdot | x_k) \approx \delta_{D_k(x_k)}$

$$D_k^y(x_k) \approx D_k(x_k) + \alpha_k^{-1}(1 - \alpha_k^2) \nabla_{x_k} \log g_0(y | D_k(x_k))$$

- Samples diverge after a few iterations

- Instead, [Chung et al. 2023] plugs  $\frac{C_k}{\|y - A(D_k(x_k))\|} \nabla_{x_k} \log g_0(y | D_k(x_k))$

- ~ 50 % more expensive in terms of memory and runtime:

$$\nabla_{x_k} \log g_0(y | D_k(x_k)) = \nabla_{x_k} D_k(x_k)^\top \nabla_{x_0} \log g_0(y | x_0)|_{x_0=D_k(x_k)}$$

[Ho, J., Salimans, T., Gritsenko, A., Chan, W., Norouzi, M. and Fleet, D.J., 2022. Video diffusion models.]

[Chung, H., Kim, J., Mccann, M.T., Klasky, M.L. and Ye, J.C., 2022. Diffusion posterior sampling for general noisy inverse problems.]

# Midpoint guidance

- Usual improvement: Gaussian approximation of  $p_{0|k}(\cdot | x_k)$ , but too expensive
- As  $\ell \rightarrow 0$ ,  $g_\ell(y | x_\ell) \approx g_0(y | D_\ell(x_\ell))$  is a more reasonable approximation
- How can it be leveraged at step  $k$  of the denoising process?

Step  $k \implies$  sample  $q_{k|0,k+1}(\cdot | \hat{D}_k^y(x_{k+1}), x_{k+1})$

[Song, J., Vahdat, A., Mardani, M. and Kautz, J., 2023, May. Pseudoinverse-guided diffusion models for inverse problems.]

[Boys, B., Girolami, M., Pidstrigach, J., Reich, S., Mosca, A. and Akyildiz, O.D., 2023. Tweedie moment projected diffusions for inverse problems.]



# Posterior backward chain

$$\begin{aligned}\pi_{0:n}^y(x_{0:n}) &= \pi_0^y(x_0) \prod_{k=0}^{n-1} q_{k+1|k}(x_{k+1} | x_k) \\ &= \pi_n^y(x_n) \prod_{k=0}^{n-1} \pi_{k|k+1}^y(x_k | x_{k+1}) \\ &\approx \mathcal{N}(0, \mathbf{I}) \quad \text{to be approximated}\end{aligned}$$

where

$$\begin{aligned}\pi_{k|k+1}^y(x_k | x_{k+1}) &= \pi_k^y(x_k) q_{k+1|k}(x_{k+1} | x_k) / \pi_{k+1}^y(x_{k+1}) \\ &= g_k(y | x_k) p_{k|k+1}(x_k | x_{k+1}) / g_{k+1}(y | x_{k+1})\end{aligned}$$

not very useful

# Midpoint decomposition

For all  $\ell \in [0 : k]$

$$\pi_{k|k+1}^y(x_k | x_{k+1}) = \int \underbrace{q_{k|\ell, k+1}(x_k | x_\ell, x_{k+1})}_{\substack{\text{Gaussian} \\ + \text{easy to sample from}}} \pi_{\ell|k+1}^y(x_\ell | x_{k+1}) dx_\ell$$

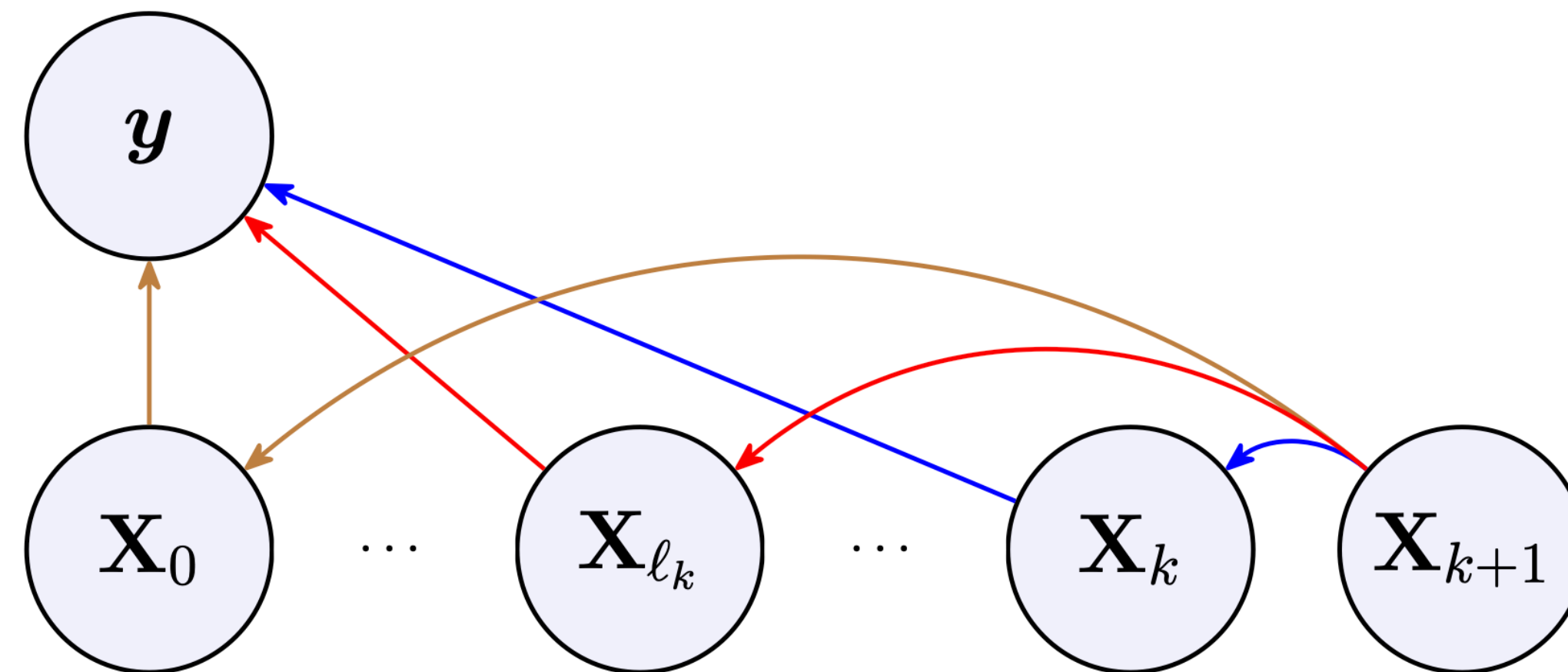
where  $\pi_{\ell|k+1}^y(x_\ell | x_{k+1}) \propto \underbrace{g_\ell(y | x_\ell)}_{\text{prior backward transition}} p_{\ell|k+1}(x_\ell | x_{k+1})$

- As  $\ell \rightarrow 0$ ,  $g_\ell(y | x_\ell) \approx g_0(y | D_\ell(x_\ell))$  is a more reasonable approximation
- But,  $p_{\ell|k+1}(x_\ell | x_{k+1}) = \int \prod_{j=\ell}^k p_{j|j+1}(x_j | x_{j+1}) dx_{\ell+1:k}$  : more **multi-modal** as  $\ell \rightarrow 0$

**There is a tradeoff!**

# Midpoint decomposition

Conditional densities involved in  $\pi_{k|k+1}^y(\cdot | x_{k+1})$  for different choices of  $\ell$



**Long** arrow  $\iff$  more difficult to approximate

# Surrogate model

Let  $(\ell_k)_{k=1}^n \in [1 : n]^n$  with  $\ell_k \leq k$ .

$$\pi_{\ell_k|k+1}^y(x_{\ell_k} | x_{k+1}) \propto g_{\ell_k}(y | x_{\ell_k}) p_{\ell_k|k+1}(x_{\ell_k} | x_{k+1})$$

For  $p_{\ell_k|k+1}(\cdot | x_{k+1})$  we use the Gaussian approximation:

$$p_{\ell_k|k+1}^\theta(x_{\ell_k} | x_{k+1}) = q_{\ell_k|0,k+1}(x_{\ell_k} | D_{k+1}^\theta(x_{k+1}), x_{k+1})$$

Surrogate backward posterior transition:

$$\hat{\pi}_{\ell_k|k+1}^\theta(x_{\ell_k} | x_{k+1}) \propto g_0(y | D_{\ell_k}^\theta(x_{\ell_k})) p_{\ell_k|k+1}^\theta(x_{\ell_k} | x_{k+1})$$

# Surrogate model

Our approximation of  $\pi$  is

$$\hat{\pi}_0^\ell(x_0) = \int \mathbf{N}(x_n; \mathbf{0}_d, I_d) \prod_{k=0}^{n-1} \hat{\pi}_{k|k+1}^\ell(x_k | x_{k+1}) dx_{1:n}$$

where

$$\hat{\pi}_{k|k+1}^\ell(x_k | x_{k+1}) = \int \underbrace{q_{k|\ell_k, k+1}(x_k | x_{\ell_k}, x_{k+1})}_{\text{straightforward to sample}} \underbrace{\hat{\pi}_{\ell_k|k+1}^\theta(x_{\ell_k} | x_{k+1})}_{\text{approximate inference}} dx_{\ell_k}$$

$$\pi_{\ell_k|k+1}^\theta(x_{\ell_k} | x_{k+1}) \propto g_0(y | D_{\ell_k}^\theta(x_{\ell_k})) p_{\ell_k|k+1}^\theta(x_{\ell_k} | x_{k+1})$$